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Multiple Liver Metastases from Carcinoma of the Thymus Treated with Yttrium-90 Radioembolization (Glass Microspheres): Clinical Dosimetry

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Abstract

Liver radioembolization with Yttrium-90 microspheres has been recognized as an emerging treatment strategy for patients with primary hepatic malignancies and metastatic liver disease. Furthermore, a shift toward the curative setting is desirable although Yttrium-90 radioembolization is primarily performed in the palliative setting.

Unfortunately, there is little information on complex patient dosimetry based on real absorbed dose distribution to the normal liver, tumor and extrahepatic tissues, from patients submitted to radioembolization.

We herein describe the case report of our first patient (multiple diffuse liver metastases failing to respond to sunitinib) submitted to radioembolization with Yttrium-90 glass microspheres at the Champalimaud Centre for the Unknown (CCU), Champalimaud Foundation (FC), focusing on complex patient clinical dosimetry based on absorbed dose calculation Stratos[®] algorithm software. This new research approach enabled to calculate the tumor liver dose to be 118 Gy very close to the pre-therapy prescribed 120 Gy. The maximum recommended normal liver dose was not reached. It was equal to 12 Gy.

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Copyright © 2016 Ferreira P. This is an open access article distributed under the Creative Commons Attribution License, which permits unrestricted use, distribution, and reproduction in any medium, provided the original work is properly cited. Keywords: Yttrium-90; ^{99m}Tc-MAA; Radioembolization; Dosimetry; Treatment planning; Dose-Volume Histogram; SPECT; PET; PET/CT

Introduction

A retrospective study is underway at the CCU, FC to investigate the delivered absorbed doses after liver Radioembolization (RE) with glass microspheres labeled with Yttrium-90 (Y90), commercially named Therasphere[®]. So far, eleven patients with multiple liver metastases have been submitted to Y90 liver RE. Quantification of absorbed doses from Positron Emission Tomography–Computed Tomography (PET/CT) images are still a matter of debate.

Herein we describe the case of a 61 years old woman, the first CCU, FC patient submitted to Y90 liver RE in January 2015. Sixteen months after the procedure, this patient is clinically well, with no evidence of metabolically active disease since January 2016.

This patient had been previously diagnosed with multifocal liver metastases from carcinoma of the thymus (c-kit positive). Past therapies included imatinib (good response) and sunitinib (initial good response and some metabolic progression thereafter). After multidisciplinary meeting discussion and based on available literature [1], she was referred for Y90 liver RE. The patient is still under imatinib after developing side effects from sunitinib.

Materials and Methods

In January 2015 diagnostic angiography was undertaken, with the intent to study liver arterial blood supply (Figure 1). During this session 274 MBq of ^{99m}Tc-MAA (macroaggregates of albumin) were injected via the main hepatic artery.

Whole body scanning and planar images of the chest and abdomen were acquired in order to calculate the percentage of possible hepato-pulmonary shunt, as requested in preparation for the RE treatment (Figure 2). This was followed by single photon emission computed tomography (SPECT)



Figure 1: Images from the perfusion scanning diagnostic angiography of our first patient treated with Y90 RE in the liver: (a) initial arterial vasculature of the liver, (b) flow shift into the diaphragmatic artery coming from hepatic branch for segment III, precluding treatment given the risk of extra hepatic migration of Y90 microspheres and thus imposing coil embolization, (c) catheter position set for coil embolization, (d) final arterial vasculature control by main hepatic artery after coil embolization, before the injection of the ^{99m}Tc-MAA via the main hepatic artery.



Figure 2: Whole body anterior and posterior images after administration of ^{99m}Tc-MAA with measurements (counts) within the regions of interest for lungs and liver used to calculate the percentage of hepato-pulmonary shunt (3% in this case).

to obtain a tomographic map of the ^{99m}Tc-MAA distribution within the liver parenchyma that is directly proportional to the intrahepatic regional arterial blood supply.

Both anterior and posterior planar images were used for the calculation of the geometric mean counts in each region of interest (ROI). The lung shunt value was then calculated based on the geometric mean of the lung counts relative to the sum of the geometric mean values of the lung and liver. The lung shunt was calculated as 3% and no other abnormal distribution of ^{99m}Tc-MAA, mainly in the abdomen outside the liver was demonstrated. The left diaphragmatic artery territory previously embolized with a coil during arteriography showed no distribution of the ^{99m}Tc-MAA.

Since there is scarce and poorly characterized information on complex dosimetry for accurate activity estimation [2-5], the prescribed Y90 activity was calculated using the classic MIRD formula [6], corrected for the lung shunt fraction (percentage of hepato-pulmonary shunt) and for recommended residual activity in the waste residue (i.e. the Y90 injector circuit after the RE procedure was terminated):

$$A = \frac{D \times m}{50 \times (1 - LSF) \times (1 - R)} \tag{1}$$

where *A* is the Y90 calculated vial activity of 2.906 GBq (gigabecquerel), *D* is the prescribed liver dose of 120 Gy (gray), *m* is the liver mass of 1.163 kg (kilograms) for 1129 cm³ (cubic centimeter) liver volume and 1.03 g.cm⁻³ of mean density of the liver tissue, *LSF* is the 0.03 (3%) lung shunt fraction and *R* is a recommended constant value of 0.01 (1%), that represents, according to the manufacturer, the residual activity not injected in patients and measured in the waste residue.

The Y90 labeled glass microspheres (Therasphere[®]) were administered according to current standard guidelines two weeks later [7]. This was carried out via injecting the microspheres into



Figure 3: Multi-modal images (same axial slice): (a) CT image with four identifiable metastases, (b) Y90 PET/CT axial image, (c) ^{99m}Tc-MAA SPECT axial image, (d) co-registration of both Y90 (PET) and ^{99m}Tc-MAA (SPECT) images. It is important to note the higher intensity of uptake for both ^{99m}Tc-MAA and Y90 microspheres corresponding to the region of the metastatic sites that appear relatively well co-registered for all three components, i.e. morphology (CT), diagnostic perfusion (MAA) and treatment (Y90-microspheres) maps.



Figure 4: VOI contours (body/orange, liver/green, right lung/blue and tumor/red) of the patient: (a) in CT images of the Y90 PET/CT series, (b) in Y90 PET/CT images.

the main hepatic artery lumen to treat both lobes of the liver. No complications or side effects were recorded during and immediately after the procedure.

Although Y90 is considered a pure electron (β -) emitter (2.28 MeV; 99.98%), its decay cascade includes a minor β - branch (518 keV; 0.017%) to the first excited state of stable Zirconium-90 (Zr90) at 1.76 MeV. This decays by gamma photon emission, originating a positron-electron (β +/ β -) pair production emission. It is this emission that is used to assess Y90 biodistribution by PET imaging [8].

Thus, after Y90 RE liver injection, PET/CT images were acquired to obtain the Y90 distribution map within the liver parenchyma for co-registration with previously acquired SPECT images from the ^{99m}Tc-MAA (Figure 3). The Y90 distribution map was also later used for patient dosimetry calculations using the Stratos[®] dosimetry calculation software (not for clinical use), a module of the Imalytics (Philips[®]) research workspace [9]. This dose calculation software is enabling us to create our own "treatment planning software" (TPS), under evaluation for subsequent implementation.

Results and Discussion

When using a TPS, the main challenge is to ensure proper calibration of the PET and SPECT images in terms of the activity measured in Becquerel per voxel intensity.

Taking into account that 1% of the Y90 calculated vial activity



Figure 5: Absorbed dose map calculated based on the pre-calibrated Y90 PET images from the patient.

remained in the injector system as residue the activity administered to the patient was 2.877 GBq. This body activity enabled the use of an iterative method within the TPS, starting with a calibration factor for PET images equal to 1 Bq/intensity, to verify the value of the activity detected in the body. Before this calculation, readjustment and confirmation of the CT and PET images co-registration was performed (Figure 3B) using the manual registration tools in the TPS. Then the segmentation tools in the TPS helped with drawing (Figure 4) all VOI contours (body, total liver, tumor, normal liver, right lung).

Finally, the dosimetry volume for absorbed dose calculation was defined in the axial, coronal and sagittal planes. Based on this dosimetry volume and Y90 injected activity (2.877 GBq) the absorbed dose was calculated. Consequently, a 3D absorbed dose map was

 Table 1: Initial VOI statistics of the calculated activity based on the pre-calibrated

 Y90 PET images from the patient.

VOI	Min	Max	Mean	Std. Dev.	Total Act.
Body	0	162	3.21	6.01	2.0x10 ⁶
LiverCCC3245	0.251	162	13.5	13.0	8.2x10⁵
normal liver	0.251	116	11.5	8.82	6.3x10⁵
right lung	0	69.3	2.03	3.47	38196
Tumor	1.25	162	34.8	25.0	1.9x10⁵
Other	0	84.5	2.10	2.95	1.1x10 ⁶

Table 2: Initial VOI statistics of the calculated absorbed dose based on the precalibrated Y90 PET images from the patient.

VOI	Min	Max	Mean	Std. Dev.
body	0	0.335	7.8x10 ⁻³	0.014
LiverCCC3245	1.1x10 ⁻³	0.335	0.033	0.029
normal liver	1.1x10 ⁻³	0.250	0.028	0.020
right lung	0	0.150	5.1x10 ⁻³	8.1x10 ⁻³
tumor	4.1x10 ⁻³	0.335	0.082	0.055
Other	0	0.182	5.1x10 ⁻³	6.4x10 ⁻³



Figure 6: Initial DVH from the absorbed dose map calculated based on the pre-calibrated Y90 PET images from the patient: (a) calculated activity, (b) calculated absorbed dose.

generated with the help of TPS (Figure 5).

For dose map quantitative analysis, we used the VOI statistics values (Table 1 and 2) and corresponding dose volume histograms (DVH) (Figure 6).

The injected activity within the body contour has been 2.877x10⁹ Bq. This originates a total intensity value of 2.0x10⁶ (given by Stratos) within the same body contour (Table 1). The calculated activity VOI statistics, assuming adequate calibration, give origin to a tumor mean dose of 0.082 a.u. (arbitrary units). For comparative purposes we may



Figure 7: Absorbed dose distribution calculated based on the calibrated Y90 PET images from the patient.

Table 3: VOI statistics of the calculated activity based on the calibrated Y90 PET images from the patient.

VOI	Min	Max	Mean	Std.Dev.	Total Act.
body	0	2.3x10⁵	4625	8643	2.9x10 ⁹
LiverCCC3245	361	2.3x10⁵	19475	18777	1.2x10 ⁹
normal liver	361	1.7x10⁵	16503	12694	9.1x10 ⁸
right lung	0	99726	2916	4996	5.5x10 ⁷
tumor	1804	2.3x10⁵	50109	35989	2.7x10 ⁸
Other	0	1.2x10⁵	3023	4244	1.6x10 ⁹

 Table 4: VOI statistics of the calculated absorbed dose based on the calibrated

 Y90 PET images from the patient.

VOI	Min	Max	Mean	Std.Dev.
body	0	481	11,3	19,9
LiverCCC3245	1,57	481	47,3	42,4
normal liver	1,57	359	40,4	28,9
right lung	0	215	7,32	11,6
tumor	5,89	481	118	79,4
Other	0	262	7,38	9,27

assume that the a.u. are directly proportional to the total calculated liver volume prescribed absorbed dose of 120 Gy. In this particular case, the activity reaching the total liver was 2.791 GBq due to the calculated hepato-pulmonary shunt (3% of the 2.877 GBq body activity).

Body activity and tumor mean dose values were confirmed by MATLAB[®] calculation based on the integral activity and dose extracted from the normalized tumor (red) curve and respective dose volume histograms (Figure 6). According to our calculations and previously mentioned assumptions we need to implement a 1439 Bq/ intensity calibration factor in the TPS dose algorithm to calculate the final activity and dose within the defined body contour.

The calibrated absorbed dose distribution is shown in Figure 7 and the related statistics are shown in Table 3 and Table 4, and in Figure 8.

The analysis of the VOI statistics of the calculated activity (Table 3), gives the total activity value for the body contour as 2.9×10^9 Bq in agreement with the expected value of 2.877 GBq. The tumor mean dose in the VOI statistics of the calculated absorbed dose (Table 4) is 118 Gy, a deviation of -1.7% from the prescribed absorbed dose of 120 Gy.

Using the proposed calibration factor we would like to emphasize that the calculated right lung Y90 activity $(5.5 \times 10^7 \text{ Bq}, \text{ Table 3})$,



Figure 8: Final DVH from the absorbed dose map calculated based on the calibrated Y90 PET images from the patient: (a) calculated activity (Bq), (b) calculated absorbed dose (Gy).

corresponds to a lung shunt value of 1.9%, one third less than the pretherapy ^{99m}Tc-MAA hepato-pulmonary shunt calculation.

The normal liver (91% of the total liver volume) mean dose (Table 4) was calculated as 40.4 Gy.

According to the presently accepted guidelines for stereotactic body radiotherapy (SBRT) [10] 700 cm³ of normal liver must be spared, i.e., the mean dose within this volume should be less than 15 Gy [11]. Based on the herein reported patient DVH (Figure 8B), the normal liver calculated mean dose is 12 Gy in 700 cm³ corresponding to 52% of total normal liver volume.

Conclusion

В

This case report illustrates several safety parameters of Y90 (Therasphere[®]) RE liver therapy in a patient with multifocal liver metastases. The patient is clinically well and free of metabolic active and FDG avid liver disease sixteen months after RE liver therapy under imatinib. Using the dose calculation Stratos[®] (Imalytics, Philips[®]) algorithm software the entire tumor volume in the liver received 118 Gy, very close to the pre-therapy prescribed 120 Gy. In our case the normal liver dose was 12 Gy in 700 cm³ that is lower than the maximum recommended normal liver dose (< 15 Gy in 700 cm³).

Final Message

In order to improve the calculation algorithms under use we have already ongoing work with the following main objectives:

- 1) to calculate calibration factors more appropriate to correct for imaging data from SPECT, PET and CT;
- 2) to improve image co-registration between modalities;

- 3) to improve automatic segmentation algorithms;
- to further evaluate the clinical "treatment planning" potential of the dose calculation software algorithms used;
- 5) to implement Monte Carlo simulation software to improve "treatment planning" dose calculation software algorithms.

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